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cont

51. (new) The laser therapy device according to claim 48, wherein the pump module optionally comprises a measuring device for calibrating internal power regulation.

52. (new). The laser therapy device according to claim 48, wherein the applicator is constructed as a handpiece for endoscopic or CPC applications.

IN THE ABSTRACT OF THE DISCLOSURE

Please add the enclosed Abstract of the Disclosure.

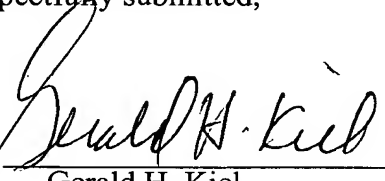
REMARKS

The specification has been amended to conform it to U.S. format and a new Abstract of the Disclosure has been added. Claims 1-26 have been cancelled and new claims 27-52 been added.

An early and favorable action on the merits is respectfully requested.

Respectfully submitted,

By:


Gerald H. Kiel
Reg. No. 25,116

April 25, 2002
REED SMITH LLP
375 Park Avenue
New York, NY 10152-1799
GHK:jl
Enc.: Substitute Specification
Abstract of the Disclosure
Preliminary Amendment



Customer No. 026418

IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

Docket No. GK-ZEI-3147 / 500343.20148

Applicant(s): Mario GERLACH, Martin WIECHMANN, Olaf KITTELMANN, Diegeo ZIMARE, Michael KEMPE Dirk MUEHLHOFF and Alexander KALIES

Application No.: 10/043,465 Group: 1398

Filed: January 10, 2002 Examiner:

For: MEDICAL LASER THERAPY DEVICE

MARKED-UP / BOLDED
VERSION OF THE
SPECIFICATION
And
ABSTRACT

Docket No.: GK-ZEI-3147/500343.20148

MEDICAL LASER THERAPY DEVICE

CROSS-REFERENCE TO RELATED APPLICATIONS

This application claims priority of German Application
No. 101 00 859.7, filed January 11, 2001, the complete disclosure of which is
hereby incorporated by reference.

10

BACKGROUND OF THE INVENTION

a) Field of the Invention

The invention is directed to a medical laser therapy device, particularly for
15 use in surgery and ophthalmology.

b) Discussion of Related Art and Problems Addressed by the Invention

In scarcely any other medical discipline is the use of lasers so established as
in ophthalmology, where patients have the very considerable advantage of
20 noninvasive treatment which can usually be performed on an outpatient basis.
Alternative methods are often unavailable or involve invasive procedures in the eye.

Almost all of the laser therapy devices currently used in ophthalmology for
photocoagulation and photodynamic therapy (PDT) comprise a laser therapy device,
an applicator and a beam control system which is usually constructed as a waveguide
25 for optical radiation and which supplies the laser radiation generated by the laser
therapy device to the applicator, through which the radiation, as therapy radiation, or
the target beam or observation beam generated by another radiation source is
directed into the eye to be treated.

Apart from Ar^+ , Kr^+ or mixed-gas lasers whose operation is very cost-
30 intensive and energy-intensive, solid-state type laser systems delivering therapeutic

MARKED-UP / BOLDED SPECIFICAATION



laser radiation of one wavelength are currently employed as radiation sources for photocoagulation and PDT. When different wavelengths of therapy radiation are required for different applications, it is generally necessary to use several laser systems or to refit existing systems in an uneconomical manner. Further, laser slit
5 lamps, with or without special link systems, of many different manufacturers are known in the art and are commercially available. These laser slit lamps are connected via a light-conducting fiber arrangement to an external (remote) laser radiation source generating an acting beam and/or target beam. Laser slit lamps of this kind are also described in patent literature and in other literature, for example,
10 US 5 921 981. In this connection, combinations of a diode laser and slit lamp or an Nd:YAG laser and slit lamp are known, for example.

The usable wavelengths of laser radiation lie in the near infrared and visible spectral regions. Optical zoom systems in the link system or applicator are used for adjusting spot sizes. Pulsed operation of the acting beam sources, for example, by
15 intensity modulation of the pump source, is also known.

The loss of radiation power occurring along the path from the radiation source through the slit lamp to the patient has turned out to be a substantial disadvantage in known laser slit lamps. In order to eliminate these disadvantages, it would be necessary to compensate for the transfer loss through higher optical and
20 electrical source outputs.

Other disadvantages include the high number of electric connection lines between the laser radiation source and the applying system (laser slit lamp), high setup costs, and long light transfer via a sensitive light-conducting fiber to the applying system (laser slit lamp or link system).

25

OBJECT AND SUMMARY OF THE INVENTION

It is the **primary** object of the invention to provide a medical laser therapy device which makes it possible to provide and apply laser radiation of different wavelengths for different applications in a simple construction by exchanging

structural component parts and/or component groups and, accordingly, to enable an effective and careful treatment of areas in or on the eye of a patient.

According to the invention, this object is **[met in different embodiment forms by the features set forth in the characterizing parts of the independent**
5 **claims 1, 4, 7, 10, 13, 16, 19 and 22. Details of the various embodiment forms are described in the corresponding subclaims] achieved by the laser therapy device described, for example, on the following page and otherwise below.**

The medical laser therapy device primarily comprises the following main components: pump module with a coupling element, laser radiation source or
10 sources, applicator and corresponding beam control system(s) which transmit(s) the laser radiation, wherein the individual main components, in turn, are constructed and positioned in different ways depending upon the application.

The laser therapy device in the embodiments comprises a controllable pump module with a suitable coupling element for a waveguide, a beam control device in
15 the form of a waveguide for supplying the pumping radiation delivered by the pump module to the laser medium and/or to the applicator, and an applicator, possibly with a coupling element for a waveguide, for introducing a target beam and/or treatment beam into the patient's eye which is to be treated.

A laser therapy device of the type mentioned above is characterized in that
20 the pump module has laser diodes whose electromagnetic pumping radiation is in the spectral range from 800 nm to 815 nm, and in that an optics module which serves as a coupling element is provided which couples the pumping radiation into the waveguide, in that the beam control device is an Nd-doped waveguide laser with a double core or single core and a suitable reflecting coating of the fiber end faces,
25 wherein the waveguide forms a laser cavity with radiation in a frequency range between 1050 nm and 1070 nm, in that the applicator is a laser slit lamp with zoom system having a device for frequency doubling which preferably comprises periodically poled nonlinear optical material, wherein this device is arranged inside or outside part of the laser cavity, and in that the applicator has a target beam device

whose radiation is coupled collinearly into the beam path for the therapy radiation by a suitable beamsplitter.

For purposes of a simpler and versatile application, it is advantageous when the applicator is constructed as a head ophthalmoscope and a device for frequency
5 doubling comprises a nonlinear optical material, known per se, this device being arrangement inside or outside the cavity. This nonlinear optical material can be a crystal.

The applicator can be constructed as a laser link with a zoom system and can comprise a device for frequency doubling which is made from nonlinear optical
10 material or periodically poled nonlinear material, wherein this device is an internal or external part of the laser cavity.

Another construction of the laser therapy device comprises a controllable pump module with a coupling element for a waveguide, a beam control device in the form of a waveguide for supplying the pumping radiation delivered by the pump
15 module to the applicator, and an applicator with a coupling element for a waveguide for introducing a target beam and/or treatment beam into the patient's eye which is to be treated. In this respect, it is advantageous when the pump module has laser diodes whose electromagnetic pumping radiation is in the spectral range from 800 nm to 815 nm, and an optics module is provided which couples the pumping
20 radiation into the waveguide, the pump module has a target beam device whose radiation is coupled into the beam path for the therapy radiation collinearly by a suitable beamsplitter, the beam control device is an Nd-doped waveguide laser with a double core or single core and suitable reflecting coating of the fiber end faces, wherein the waveguide forms a laser cavity with radiation in a frequency range
25 between 1050 nm and 1070 nm, the applicator is a laser slit lamp with a zoom system which has a device for frequency doubling comprising nonlinear optical material or periodically poled nonlinear optical material, the applicator has a device for power monitoring and a device for illuminating and observing the operating field.

It is further advantageous that the applicator is a head ophthalmoscope which has a device for frequency doubling preferably comprising nonlinear optical material which can also be periodically poled, wherein this device is an internal or external part of the laser cavity.

5 The applicator can also be a laser link which has a zoom system and a device for frequency doubling preferably comprising nonlinear optical material which can also be periodically poled, wherein this device can be an internal or external part of the laser cavity.

 Another embodiment form of a laser therapy device, according to the
10 invention, **[with the preamble of claim 7]** is characterized in that the pump module comprises laser diodes whose electromagnetic pumping radiation is in the spectral range from 830 nm to 850 nm, in that an optics module is provided which couples the pumping radiation of the laser diodes into the waveguide, in that the beam control device is constructed as a Pr/Yb-doped waveguide with suitable reflecting
15 coating of the fiber end faces, so that the waveguide forms a laser cavity for radiation in the frequency range between 520 nm and 540 nm or between 630 nm and 640 nm, depending on its technical design, in that the applicator is a laser slit lamp with a zoom system, comprises a device for monitoring power and a device for illuminating and observing the operating field, and in that the applicator has a target
20 beam device whose radiation is coupled into the beam path for the therapy radiation collinearly by a beamsplitter.

 In this case also, the applicator can be constructed as a head ophthalmoscope or as a laser link with zoom system.

 Another construction of a therapy device which meets the stated object of the
25 invention is characterized in that the pump module comprises laser diodes whose electromagnetic pumping radiation is in the spectral range from 830 nm to 850 nm, and in that an optics module is provided which couples the radiation of the laser diodes into the waveguide, in that the beam control device is constructed as a Pr/Yb-doped waveguide with suitable reflecting coating of the fiber end faces, so that the
30 waveguide forms a laser cavity for radiation in the frequency range between 520 nm

and 540 nm or between 630 nm and 640 nm, depending on its technical design, in that the applicator is a laser slit lamp with a zoom system, comprises a device for monitoring power and a device for illuminating and observing the operating field, and in that the pump module comprises a target beam device whose radiation is
5 coupled into the beam path for the pumping radiation collinearly by a beamsplitter.

In this connection, it is advantageous when the applicator is a laser slit lamp with a zoom system or a head ophthalmoscope.

The applicator can also advantageously be a laser link with zoom system.

A therapy device which also meets the above-stated object [**according to the**
10 **preamble of claim 13]**is characterized in that the pump module comprises laser diodes whose electromagnetic pumping radiation is in the spectral range from 970 nm to 980 nm, and in that an optics module is provided which couples the pumping radiation of the laser diodes into the fiber, in that the beam control device is constructed as an Er-doped waveguide with suitable reflecting coating of the
15 waveguide end faces, so that the waveguide forms a laser cavity for radiation in the frequency range between 540 nm and 550 nm, in that the applicator is a laser slit lamp with a zoom system, in that the applicator comprises a device for monitoring power, in that the applicator comprises a device for illuminating and observing the operating field, and in that the applicator comprises a target beam device whose
20 radiation is coupled into the beam path for the therapy radiation collinearly by a beamsplitter.

In this case, the applicator is also advantageously a head ophthalmoscope or a laser link with zoom system.

In another modification of a laser therapy device according to the invention,
25 it is advantageous that the pump module comprises laser diodes whose electromagnetic pumping radiation is in the spectral range from 970 nm to 980 nm and that an optics module is provided which couples the pumping radiation of the laser diodes into the fiber, the beam control device is constructed as an Er-doped waveguide with suitable reflecting coating of the waveguide end faces, so that the
30 waveguide forms a laser cavity for radiation in the frequency range between 540 nm

and 550 nm, the applicator is a laser slit lamp with a zoom system, the applicator comprises a device for monitoring power and a device for illuminating and observing the operating field, and the pump module comprises a target beam device whose radiation is coupled into the beam path for the pumping radiation collinearly
5 by a suitable beamsplitter.

In this device, also, the applicator is advantageously a laser slit lamp with zoom system. However, it can also be constructed as a head ophthalmoscope.

Further, the applicator can be a laser link with zoom system.

Another laser therapy device, constructed according to the invention, for
10 medical applications comprises a controllable pump module with a coupling element for a waveguide, a beam control device in the form of a waveguide for supplying the pumping radiation delivered by the pump module to the applicator, and an applicator with a coupling element for the waveguide for introducing a target beam and/or treatment beam into the patient's eye which is to be treated. The therapy device is
15 further characterized in that the pump module has laser diodes whose electromagnetic pumping radiation is in the spectral range from 800 nm to 815 nm, and in that an optics module is provided which couples the pumping radiation into the waveguide, in that the beam control device is a non-doped waveguide, possibly with antireflection-coated end faces, so that the pumping radiation is supplied to the
20 applicator, in that the applicator is a laser slit lamp with zoom system which comprises a microchip laser for converting the pumping radiation into radiation in the green spectral range, in that the applicator has a device for monitoring power and a device for illuminating and observing the operating field, and in that the applicator has a target beam device whose radiation is coupled into the beam path for the
25 therapy radiation collinearly by a beamsplitter.

Accordingly, it is advantageous that the applicator is a head ophthalmoscope which comprises a microchip laser for converting the pumping radiation into radiation in the green spectral range.

The applicator can also be a laser link with a zoom system and with a microchip laser for converting the pumping radiation into radiation in the green spectral range.

According to another construction of the invention, **[according to the**
5 **features of the preamble of claim 22]** the following characterizing features are provided:

the pump module comprises laser diodes whose electromagnetic pumping radiation is in the spectral range from 800 nm to 815 nm, and an optics module is provided which couples the pumping radiation into the waveguide; the beam control
10 device is a non-doped waveguide, possibly with antireflection-coated end faces, so that the pumping radiation is supplied to the applicator; the applicator is a laser slit lamp with zoom system which comprises a microchip laser for converting the pumping radiation into radiation in the green spectral range; the applicator has a device for monitoring power and a device for illuminating and observing the
15 operating field; the pump module has a target beam device whose radiation is coupled into the beam path for the pumping radiation collinearly by a suitable beamsplitter; the applicator is a laser slit lamp with zoom system which comprises a microchip laser for converting the pumping radiation into radiation in the green spectral range.

20 In this connection, the applicator is advantageously a head ophthalmoscope which comprises a microchip laser for converting the pumping radiation into radiation in the green spectral range.

The applicator can also be a laser link with zoom system which comprises a microchip laser for converting the pumping radiation into radiation in the green
25 spectral range.

For purposes of a versatile, all-purpose application of the laser therapy device, it is particularly advantageous when the applicator is constructed as a handpiece for endoscopic or CPC applications to which is connected a beam control device in the form of a waveguide.

Generally, it is advantageous in all applications when the pump module optionally comprises a measuring device for calibrating internal output regulation.

The invention will be explained more fully in the following with reference to embodiment examples.

5

BRIEF DESCRIPTION OF THE DRAWINGS

In the drawings, Figs. 1 to 9 show schematic block diagrams of different embodiment examples of a medical therapy device in modular construction.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

10 Identical elements and identical component groups are identified by identical reference numbers in the individual Figures. The examples are described with reference to an applicator with slit lamp. Instead of the slit lamp, a head ophthalmoscope, a link system or a correspondingly constructed handpiece can also be used.

15 The medical laser therapy device, in particular for application in ophthalmology, which is illustrated as a block diagram in Fig. 1 comprises a pump module PM which, in turn, comprises a pumping radiation source PQ emitting pumping radiation in a wavelength range from 780 nm to 815 nm. This pump module PM is connected, preferably by a coupling element (not shown), to a
20 waveguide laser WLL which emits radiation in the wavelength range from 1050 nm to 1070 nm and which is a beam control device in the form of a single-core or double-core waveguide, known per se. This waveguide comprises a core of material which is doped with laser-active ions Nd^{3+} , the end faces of the waveguide being constructed as a cavity mirror corresponding to the wavelength of the radiation.

25 The radiation emitted by the waveguide laser WLL is supplied to an applicator AP which is arranged downstream, possibly with the intermediary of a suitable coupling element (not shown in Fig. 1), and which can be constructed in various ways. In Fig. 1, it is shown as a block identified by a dash-dot line. The applicator AP further includes a frequency doubler FD comprising a nonlinear,
30 optical crystal, known per se, which doubles the frequency of the laser radiation and

which is arranged downstream of the waveguide laser WLL, and a slit lamp SL with a slit lamp microscope and zoom system ZS and a device LÜ for measuring and monitoring the power of the emitted radiation.

In this embodiment form of the therapy device according to the invention, the slit lamp SL comprises a target beam device ZE which emits a target beam for targeting the location to be treated in or on the eye A, this target beam being coupled into the beam path for the therapy radiation collinearly by deflecting means 1 and a suitable beamsplitter 2. Accordingly, it is always ensured that the target beam and therapy beam strike the location to be treated in or on the eye A together. In other arrangements, it may be advantageous to unite the illumination in noncollinear fashion with the therapy beam in the operating field in order to prevent impairment of the therapy beam by the beamsplitter 3.

As can be seen further from Fig. 1, the applicator AP comprises an illumination beam source BQ whose emitted radiation is coupled into the beam path 4 exiting the applicator AP collinearly via another beamsplitter 3. In this way, an illumination of the location to be irradiated is also realized, so that a visual observation is also made possible through the slit lamp microscope.

The provided zoom system ZS serves to change the cross section of the therapy beam and, therefore, the adjustment of the spot size on the irradiated location. It is also advantageous when the applicator AP has an arrangement for power monitoring LÜ of the delivered radiation.

The applicator AP itself can be constructed as a slit lamp SL or as a head ophthalmoscope, link system or handpiece.

The therapy device according to Fig. 1 can also comprise an Er-doped waveguide laser WLL which is pumped by a pumping radiation of wavelengths between 970 nm and 980 nm and which emits radiation in the range from 540 nm to 550 nm.

In the laser therapy device shown in Fig. 2, a pumping radiation source PQ which emits a radiation in the range from 830 nm to 850 nm is provided in the pump module. The waveguide laser WLL which is provided as therapy radiation source

has an Nd/Pr-doped fiber core and emits radiation in the visible wavelength range from 520 nm to 540 nm or 630 nm to 640 nm, so that frequency doubling of the radiation is obviated and a frequency doubler is not provided.

Aside from the pumping radiation source PQ, the pump module PM in the
5 therapy device according to Fig. 3 also comprises the target beam device ZE whose radiation is coupled into the pumping beam by a deflecting mirror 5 and a beamsplitter 6 and conveyed further into the Nd-doped waveguide laser WLL. The wavelength of the waveguide laser WLL is 1050 nm to 1070 nm and the wavelength of the pumping radiation is in the range from 780 nm to 815 nm. Since the
10 wavelength of the radiation emitted by the waveguide laser WLL is not in the visible region of the spectrum, a frequency doubler FD is arranged in the applicator AP downstream of the laser. The slit lamp SL comprises the zoom system ZS and the device for power monitoring LÜ. The beam of the illumination radiation source BQ is coupled into the beam path 4 by the beamsplitter 3 and is further conveyed into the
15 eye A; this in-coupling can be carried out in collinear or non-collinear manner.

In the device according to Fig. 4, the device for power monitoring LÜ and the pumping radiation source PQ are arranged in the pump module PM. The target beam device ZE is located in the slit lamp SL which is a component part of the applicator AP. The pumping radiation source PQ emits radiation in the range from
20 780 nm to 815 nm. The waveguide laser WLL is Nd-doped. Its emitted therapy radiation has wavelengths from 1050 nm to 1070 nm; therefore, a frequency doubler FD is arranged after it. As in the device according to Figures 1 to 3, the zoom system ZS is located in the slit lamp SL. The illumination radiation source BQ is arranged in the applicator AP. Its radiation is again coupled into the beam path 4
25 through the beamsplitter 3. This can be carried out in collinear or non-collinear manner.

In the therapy device shown in Fig. 5, the pump module PM comprises the pumping radiation source PQ, the target beam device ZE and the device for power monitoring LÜ. The target beam is coupled into the pumping beam by the deflecting
30 mirror 5 and the beamsplitter 6. The pumping radiation source PQ emits radiation in

the range from 780 nm to 815 nm. The waveguide laser WLL is doped with Nd. The therapy radiation emitted by it has wavelengths from 1050 nm to 1070 nm; therefore, a frequency doubler VD is arranged after it. The zoom system ZS is arranged in the slit lamp SL. Aside from the frequency doubler VD, the applicator
5 AP also comprises the slit lamp SL and the illumination radiation source BQ and the beamsplitter 3.

Fig. 6 shows a medical therapy device with a pump module PM which is constructed identical to the module shown in Fig. 3. The pumping radiation source PQ emits a pumping radiation in the wavelength range from 830 nm to 850 nm. The
10 radiation of the Pr/Yb-doped waveguide laser WLL is in the range from 520 nm to 540 nm or 630 nm to 640 nm, depending on its technical construction. With this device it is also possible, for example, to provide a pumping radiation source PQ with pumping radiation of a wavelength of 970 nm to 980 nm and to provide an Er-doped waveguide laser WLL which emits radiation in a wavelength range from 540
15 nm to 550 nm. The applicator AP comprises the slit lamp SL with zoom system ZS, the illumination radiation source BQ and the device for power monitoring LÜ. The light of the illumination radiation source BQ is also coupled into the beam path 4 in a collinear or non-collinear manner by the beamsplitter 3.

The medical therapy device according to Fig. 7 comprises a pump module
20 PM with the pumping radiation source PQ and the device for power monitoring LÜ. The pumping radiation source PQ emits a pumping radiation in the wavelength range from 830 nm to 850 nm. The radiation of the Pr/Yb-doped waveguide laser WLL is in the range from 520 nm to 540 nm or 630 nm to 640 nm. With this device it is also possible, for example, to provide a pumping radiation source PQ with
25 pumping radiation of a wavelength of 970 nm to 980 nm and to provide an Er-doped waveguide laser WLL which emits radiation in a wavelength range from 540 nm to 550 nm. A frequency doubler is not required in this construction. The target beam device ZE is located in the slit lamp SL. The deflecting means 1 and the beamsplitter 2 are provided for collinear coupling of the target beam into the therapy
30 beam and are arranged in front of the zoom system ZS in the radiating direction.

The zoom system ZS is likewise arranged in the slit lamp SL. In this case, the illumination radiation is coupled into the beam path exiting the applicator AP in the manner described further above.

5 The therapy device shown in Fig. 8 as a block diagram differs from that shown in Fig. 5 only in that there is no frequency doubler in the device according to Fig. 8. Such a frequency doubler is also not required, since the waveguide laser WLL emits radiation in a wavelength range that is favorable and required for therapy, so that frequency doubling can be dispensed with. The pumping radiation source PQ emits a pumping radiation in the wavelength range from 830 nm to 850
10 nm. The radiation of the Pr/Yb-doped waveguide laser WLL is in the range from 520 nm to 540 nm or 630 nm to 640 nm. With this device it is also possible, for example, to provide a pumping radiation source PQ with pumping radiation of a wavelength of 970 nm to 980 nm and to provide an Er-doped waveguide laser WLL which emits radiation in a wavelength range from 540 nm to 550 nm. As concerns
15 the rest of the construction, reference is had to the description relating to Fig. 5.

For purposes of a versatile, all-purpose application of the laser therapy device, it is particularly advantageous when the applicator is constructed as a handpiece for endoscopic or CPC applications, a beam control device in the form of a waveguide being connected to this handpiece.

20 Generally, it is advantageous in all applications when the pump module optionally comprises a measuring device for calibrating the internal power regulation.

The medical therapy device according to the invention is constructed in modular manner and makes it possible to provide and apply laser radiation of
25 different wavelengths for different applications in a simple construction by exchanging structural component parts and/or component groups and, accordingly, to enable an effective and careful treatment particularly of areas in or on the eye of a patient.

While the foregoing description and drawings represent the present
30 **invention, it will be obvious to those skilled in the art that various changes may**

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be made therein without departing from the true spirit and scope of the present invention.

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